Does the CO₂ laser reduce bond strength in different types of ceramic brackets?

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Objective: The aim of this study was to assess *in vitro* the influence of the CO_2 laser and of the type of ceramic bracket on the shear bond strength (SBS) to enamel.

Methods: A total of 60 enamel test surfaces were obtained from bovine incisors and randomly assigned to two groups, according to the ceramic bracket used: Allure (A); Transcend (T). Each group was divided into 2 subgroups (n=15): L, laser (10W, 3s); C, no laser, or control. Twenty-four hours after the bonding protocol using Transbond XT, SBS was tested at a crosshead speed of 0.5 mm/min in a universal testing machine. After debonding, the Adhesive Remnant Index (ARI) was evaluated at 10x magnification and compared among the groups. Data were analyzed by one-way ANOVA, Tukey's, Mann-Whitney's and Kruskal-Wallis tests ($\alpha = 0.05$).

Results: Mean SBS in MPa were: $AL=0.88\pm0.84$; $AC=12.22\pm3.45$; $TL=12.10\pm5.11$; $TC=17.71\pm6.16$. ARI analysis showed that 73% of the specimens presented the entire adhesive remaining on the tooth surfaces (score 3). TC group presented significantly higher SBS than the other groups. The lased specimens showed significantly lower bond strength than the non-lased groups for both tested brackets.

Conclusion: CO, laser irradiation decreased SBS values of the polycrystalline ceramic brackets, mainly Allure.

Keywords: Carbon dioxide. Dental debonding. Lasers. Orthodontic brackets. Shear strength.

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INTRODUCTION

The use of ceramic brackets has become widespread in orthodontic treatments due to the increased number of adult patients seeking care and esthetic appliances.¹ However, compared to conventional metallic brackets, ceramic brackets are more costly, with a questionable clinical performance, since their rigid properties may cause antagonist tooth contact wear. Also, conventional methods for debonding ceramic brackets (pliers and drills) can cause injuries and fractures to the enamel.²⁻⁵ The difficulties for debonding ceramic brackets can be attributed to the high bond strength and to the low fracture strength of ceramics,^{5,6} which can lead to iatrogenic enamel damages, bracket fractures and longer clinical chairtime.¹⁻⁶

Therefore, several techniques were suggested for debonding of ceramic brackets, such as electrothermal devices,⁷ ultrasound,⁸ solvents⁹ and recently the lasers.^{5,10-17} The use of electrothermal devices has been an effective method in debonding ceramic brackets, however, due to irreversible heating damages to the pulp, this device lost popularity among the clinicians.⁷

The laser debonding technique is based on controlled thermal softening of the adhesive resin that leads to adhesion strength degradation. Studies have shown no pulp damage when debonding brackets with a laser device.^{5,10,11,18}

In this way, despite the good results obtained with different types of lasers, carbon dioxide (CO_2) laser has been considered the best choice for removing ceramic brackets, due to the high absorption of its wavelength in ceramic surfaces.^{14,15}

There are several variables in the studies concerning ceramic bracket removal by lasers, such as: laser settings, type of brackets and bonding agents, as well as the employed methodology. Therefore, in view of the increased use of ceramic brackets in orthodontic patients and the improvements in laser technology and adhesive dentistry in dental practice, the aim of the current investigation was to assess *in vitro* the influence of CO_2 laser use and of the type of ceramic bracket on the shear bond strength (SBS) to enamel. The null hypothesis tested was that the CO_2 laser irradiation does not decrease SBS values of the evaluated polycrystalline ceramic brackets.

MATERIAL AND METHODS

This study had no need to be submitted to an ethics committee in animal experimentation, since the samples were product of commercial slaughter of animal.

Recently extracted sound bovine permanent mandibular incisors were immersed in 0.1% thymol solution at 4°C for 1 week. Prior to use, the teeth were hand scaled, cleaned with pumice-water slurry using Robinson bristle brushes in a low-speed handpiece and examined with a stereomicroscope (Nikon Inc. Instrument Group, Melville, NY, USA) at 10x magnification to discard those with cracks, fractures or structural abnormalities that could interfere in the results. Sixty bovine teeth were selected, thoroughly washed in running water to eliminate storage solution traces, and maintained in distilled water at 4°C. The samples followed the ISO TR11405¹⁹ instructions, that recommend 15 teeth per group for shear bond strength tests.

The crowns were embedded in chemically activated acrylic resin (Jet Clássico, São Paulo/SP, Brazil) and after resin polymerization, the buccal enamel surfaces were flattened with #400- to #1200-grit silicon carbide (SiC) papers (Buehler Ltd., Lake Bluff, IL, USA) in a low-speed polishing machine (Politriz DP-9U2; Struers, A/S, Copenhagen, Denmark) in order to obtain the test sites that, for standardization, were demarcated by attaching a piece of insulating tape with a central square (5×5 mm) on each surface. Next, the roots were embedded in chemically activated acrylic resin (Jet Clássico, São Paulo/SP, Brazil) using polyvinyl chloride rings (2.1 cm diameter and 1.1 cm high) in order to facilitate the laser irradiation and the SBS test immediately after.

The 60 enamel test surfaces were randomly assigned to two groups (n=30), according to the used polycrystalline ceramic bracket: A) Allure (GAC, New York, NY, USA), and T) Transcend (3M Unitek, Monrovia, CA, USA).

Prior to the bracket bonding protocol, the test surfaces were cleaned by rubber cup/pumice prophylaxis for 10 s, rinsed and dried for the same time with an oilfree air stream. Next, the enamel surfaces were etched with 37% phosphoric acid gel (ScotchBond etchant, 3M/ESPE, St. Paul, MN, USA) for 15 s, rinsed thoroughly for 15 s, dried with a mild, oil-free air stream to obtain a uniformly white, opaque, chalk-like appearance. Transbond XT primer (3M Unitek, Monrovia, Romano FL, Pessoti G, Galo R, Gomes-Silva JM, Lucisano MP, Borsatto MC, Nelson-Filho F

The ceramic brackets for lower central incisor were bonded to the center of the specimens using Transbond XT composite (3M Unitek, Monrovia, CA, USA) according to the manufacturer's recommendations. All bonding procedures were performed by the same operator, who used a pair of pliers (Ortoply, Philadelphia, PA, USA), and the excess of material was removed with a sharp explorer (Duflex, Juiz de Fora/MG, Brazil). Each bracket bonding was photoactivated at a 1 mm distance between the bracket base and the light-curing device for 40s (10s for each side of the bracket) with a visible light curing unit (XL 1500; 3M/ESPE, St. Paul, MN, USA) with a 450 mW/cm² output power. Light intensity of each device was measured prior to each photo-activation cycle using a curing radiometer (Demetron, Danbury, CT, USA). Then the specimens were randomly divided into two subgroups (n=15): Laser (L) and No Laser, or control (C). The specimens were stored in distilled water at 37 °C for 24 h.

Immediately before the SBS test, the samples in the laser group were irradiated. The equipment used for CO_2 laser irradiation was a UM-L30 device (Shangai-Jue Hua Technology Development Shangai, PR China) emitting at 10.6µm wavelength. The laser beam was delivered in non-contact mode. The laser tip was held perpendicularly at a 4-mm distance from the bracket surface and the light was delivered in focused mode. The parameter settings were 10 W for 3s. The laser operated at ultra-pulse mode with pulse duration of 100 µs (interval time: 0,01s). The time delay between laser irradiation and force application was up to $3s^{17}$.

The SBS was tested to failure using a knife-edge blade in a universal testing machine (Model DL 500, EMIC Ltda., São José dos Pinhais/PR, Brazil) running at a crosshead speed of 0.5 mm/min with a 50 kgf load cell (Fig 1).

Mean SBS values (in MPa) and standard deviations were calculated and data were analyzed statistically by one-way ANOVA. Tukey's test was used for multiple comparisons at 5% significance level.

The debonded specimens were observed with a 10x stereomicroscope (Carl Zeiss, Goettingen, Germany) by an calibrated and experienced examiner, in order to assess the amount of resin material adhered to enamel



Figure 1 - Specimen with the active chisel tip acting on the upper part of the bracket base during the shear bond strength test.

after bracket removal, which were classified according to the Adhesive Remnant Index (ARI) scores established by Artun and Bergland:²⁰ 0 = no adhesive remaining adhered to enamel; 1 = less than half of the adhesive remaining adhered to enamel; 2 = more than half of the adhesive remaining adhered to enamel; 3 = all the adhesive remaining adhered to enamel. All examinations were done by a single examiner blinded to the groups to which the specimens belonged. The ARI scores data were statistically analyzed by the Kruskal-Wallis test and Mann-Whitney complementary test, at a significance level of 5%.

RESULTS

SBS means (in MPa), standard deviation, and statistical analysis are presented in Table 1. Group TC presented the highest and group AL present the lowest SBS values of all groups (p < 0.05), respectively. There was no statistically significant difference between groups AC and TL. Nevertheless, the SBS values were statistically lower in the CO₂ laser irradiated specimens for both Allure and Transcend tested ceramic brackets.

Statistically significant difference (p < 0.05) was found in the ARI scores among the four groups. ARI scores are illustrated in Figure 2. According to the results, 73% of the specimens presented ARI score 3, indicating that bond failure occurred predominantly at the bracket–adhesive interface, leaving most of the adhesive on the enamel surface. ARI score 0 was only observed in one specimen of TL group.

Table 1 - Comparison of shear bond strength means values (MPa).

| Groups | n | Mean (SD) | Tukey's test* |
|--------|----|--------------|---------------|
| AC | 15 | 12.22 (3.45) | a |
| AL | 15 | 0.88 (0.84) | b |
| ТС | 15 | 17.71 (6.16) | С |
| TL | 15 | 12.10 (5.11) | а |

* Same letters indicate no statistically significant difference.

AC = Allure Control; AL = Allure Laser; TC = Transcend Control; TL = Transcend Laser.

Table 2 - Comparison of ARI scores by p values (Mann-Whitney test).

| Groups | AC | AL | тс | TL |
|--------|--------|--------|--------|--------|
| AC | | 0.029* | 0.011* | 0.000* |
| AL | 0.029* | | 0.000* | 0.000* |
| TC | 0.011* | 0.000* | | 0.000* |
| TL | 0.000* | 0.000* | 0.000* | |

*Changes are significant at p < 0.05.

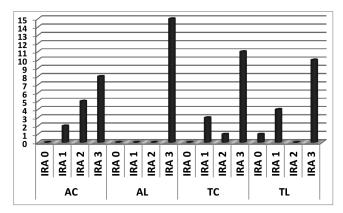


Figure 2 - ARI scores after bracket debonding.

DISCUSSION

Recently, Orthodontics experienced a great scientific advance regarding the improvement of materials and techniques, allowing more esthetic treatments. Ceramic brackets offer esthetics, durability and better color stability. Nevertheless, enamel cracks and fractures or bracket breakage due to the brittleness, low ductility, high elastic modulus and high adhesion strength to teeth of ceramics have been observed in the conventional debonding of these appliances.^{1,3} According to some authors, laser debonding of ceramic brackets eliminates damages to enamel by reducing the required force to remove it.^{13,14,18,21} The lasers act softening the adhesive bonding agent by heat conductivity.^{11,21} Saito et al.²² concluded that ceramic bracket debonding with CO_2 laser, when adhesives containing thermal expansion microcapsules are used, can be an effective and safe method. CO_2 laser has been considered the favorite laser device for debonding ceramic brackets since its wavelength is more easily absorbed by these brackets.^{14,15} In the present research, the CO_2 laser irradiation decreased the force required to remove the polycrystalline ceramic brackets.

Studies have reported no pulp or enamel tissue injuries and also a decreased debonding force and operation time with CO_2 laser.^{11,15} Lijima et al.¹⁰ have observed that the hardness and elastic modulus of enamel are not affected by CO_2 laser irradiation. Nevertheless, the workable laser parameters are directly related to the lasers' ability to soften the adhesive resin without adversely affecting tooth tissues.

The laser settings applied (10W/3s) in this study were based on the findings of a previous investigation done by this research group, in which these CO₂ laser parameters did not increase the intrapulpal temperature above the pulp physiologic tolerance.¹⁷ The employed ultra-pulse CO_2 laser can provide short pulses with sufficient time to permit tooth tissues to cool down between pulses.¹⁵ Obata et al.¹¹ have shown that CO_2 laser at 3W/3s are safe settings when debonding brackets, while other authors²³ reported that CO_2 laser irradiation at 50 w for 2 s increased 0.70°C in pulp chamber temperatures. Yassaeiet al.⁵ found a 1.46°C increase in intrapulpal temperature after diode laser irradiation at 2.5 W for 10 s.

As regards as the type of bracket, ceramic brackets are constituted by alumina and are monocrystalline (sapphire) or polycrystalline structures. The monocrystalline ceramic brackets show greater strength, but the fracture resistance is generally below that of the polycrystalline brackets.^{24,25} Also, monocrystalline brackets require lower laser energy for debonding than the polycrystalline brackets²¹ since polycrystalline units do not allow high transmissibility, thus increasing energy loss.²⁶ Thus, in the present study, polycrystalline brackets were used and higher values of SBS were observed for the Transcend ceramic brackets, which might be attributed to differences in the base design, structure, and composition of the tested brackets. Perhaps if other laser parameters were used, different SBS values would be reported.

Under clinical conditions, adequate bracket bond strength values might be between 6 to 8 MPa in order to prevent risk of tooth damages at debonding.²⁷ However, the force required to remove ceramic brackets can reach values of 20 MPa, which might cause tooth or bracket fractures by exceeding the cohesive strength of the enamel or the bracket.^{2,3,27} Confirming these facts, in this study, Transcend ceramic bracket reached a SBS mean of 17.71 MPa, which is much higher than the ideal bracket bond strength value.

Additionally, even though the laser decreased the ceramic brackets bond strength, only for the Allure group this reduction (93%) reached clinically applicable values for debonding (0.88 MPa). The Transcend lased group showed a reduction in 68%, but SBS values (12.10 MPa) were still near the limit of force (11.1 MPa) that can cause tooth fractures at debonding.²⁸ In the different treatments (with laser or without laser), the adhesion of Transcend ceramic brackets were higher than Allure. However, significant reduction in the adhesion with both brackets was observed when laser was applied. Ma et al.¹⁸ have observed that specimens debonded with CO_2 laser (18W/2s) were only 25% (1.48 MPa) of the mean of the non-lased group. Other authors¹⁰ reported that CO_2 laser irradiated specimens showed a 31% decrease in SBS, if they were bonded with a conventional etch and rinse adhesive system, and a 25% decrease with a self-etching adhesive system, compared with control (non-irradiated) specimens. However, these studies tested other materials and techniques.

Concerning ARI scores, the fractures after bracket debonding occurred predominantly at the bracket/ resin interface (73%, score 3), which reduces the risk of bracket or tooth damages.²⁹ ARI scores 1 and 2 occurred as the SBS increased and score 0 was observed only in one TL group specimen, situation in which cracking of the enamel is more probable.28 These findings suggest that, in addition to softening, the adhesive resin might have undergone thermal ablation and photoablation, resulting in vaporization and decomposition of the material.¹ The high percentage of score 3 (all composite remain after debonding) indicated that laser irradiation didn't cause injuries or fractures in the enamel surface, preserving the dental structure (Fig 2). In groups 1, 3 and 4, this score was predominant and in group 2, all sample obtained this same result. These results are promising, and probably during laser irradiation procedure a slight softening of the composite occurred, without heating the tooth.

In view of the above considerations and based on findings of the current investigation, the CO_2 laser has been noted as a promising technology in debonding ceramic brackets, mainly for the Allure, since it was observed a greater adhesive remnant index on the tooth surface together with decreased SBS values.

There is still much to be investigated concerning specific laser parameters for the adhesive resins and ceramic brackets available for orthodontic treatment, in order to justify the use of such protocols in clinical orthodontic practice. As regards time saving, lower complexity of treatment, decreased damages to tooth structures and discomfort, the use of lasers for debonding esthetic ceramic brackets has a significant advantage over the traditional method. The lack of reported studies testing the same methodology and materials used in the present study did not allow a reliable comparison with the outcomes of previous researches.

CONCLUSION

The null hypothesis was rejected. The CO_2 laser irradiation decreased the adhesion of the ceramic brackets and enhanced brackets debonding.

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Authors contribution

Conception or design of the study: FLR, MCB, PNF. Data acquisition, analysis or interpretation: GP, MPL, RG. Writing the article: FLR, JMGS. Critical revision of the article: FLR, PNF. Final approval of the article: FLR. Obtained funding: GP.

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